

FORM PTO-1390 (Modified)
(REV 11-98)

U.S. DEPARTMENT OF COMMERCE PATENT AND TRADEMARK OFFICE

ATTORNEY'S DOCKET NUMBER

TRANSMITTAL LETTER TO THE UNITED STATES
DESIGNATED/ELECTED OFFICE (DO/EO/US)
CONCERNING A FILING UNDER 35 U.S.C. 371

A33846-PCT USA

U.S. APPLICATION NO. (IF KNOWN, SEE 37 CFR

09/719960

INTERNATIONAL APPLICATION NO.

PCT/GB99/01884

INTERNATIONAL FILING DATE

18 June 1999

PRIORITY DATE CLAIMED

18 June 1998

TITLE OF INVENTION

REACTION MONITORING SYSTEM

APPLICANT(S) FOR DO/EO/US

HAGERLID, Peter; EKSTROM, Bjorn; and SJOBERG; Jonas

Applicant herewith submits to the United States Designated/Elected Office (DO/EO/US) the following items and other information:

1. ☒ This is a **FIRST** submission of items concerning a filing under 35 U.S.C. 371.
2. ☐ This is a **SECOND** or **SUBSEQUENT** submission of items concerning a filing under 35 U.S.C. 371.
3. ☒ This is an express request to begin national examination procedures (35 U.S.C. 371(f)) at any time rather than delay examination until the expiration of the applicable time limit set in 35 U.S.C. 371(b) and PCT Articles 22 and 39(1).
4. ☒ A proper Demand for International Preliminary Examination was made by the 19th month from the earliest claimed priority date.
5. ☒ A copy of the International Application as filed (35 U.S.C. 371 (c) (2))
 - a. ☒ is transmitted herewith (required only if not transmitted by the International Bureau).
 - b. ☐ has been transmitted by the International Bureau.
 - c. ☐ is not required, as the application was filed in the United States Receiving Office (RO/US).
6. ☐ A translation of the International Application into English (35 U.S.C. 371(c)(2)).
7. ☒ A copy of the International Search Report (PCT/ISA/210).
8. ☒ Amendments to the claims of the International Application under PCT Article 19 (35 U.S.C. 371 (c)(3))
 - a. ☐ are transmitted herewith (required only if not transmitted by the International Bureau).
 - b. ☐ have been transmitted by the International Bureau.
 - c. ☐ have not been made; however, the time limit for making such amendments has NOT expired.
 - d. ☒ have not been made and will not be made.
9. ☐ A translation of the amendments to the claims under PCT Article 19 (35 U.S.C. 371(c)(3)).
10. ☐ An oath or declaration of the inventor(s) (35 U.S.C. 371 (c)(4)).
11. ☒ A copy of the International Preliminary Examination Report (PCT/IPEA/409).
12. ☐ A translation of the annexes to the International Preliminary Examination Report under PCT Article 36 (35 U.S.C. 371 (c)(5)).

Items 13 to 20 below concern document(s) or information included:

13. ☐ An Information Disclosure Statement under 37 CFR 1.97 and 1.98.
14. ☐ An assignment document for recording. A separate cover sheet in compliance with 37 CFR 3.28 and 3.31 is included.
15. ☒ A **FIRST** preliminary amendment.
16. ☐ A **SECOND** or **SUBSEQUENT** preliminary amendment.
17. ☐ A substitute specification.
18. ☐ A change of power of attorney and/or address letter.
19. ☒ Certificate of Mailing by Express Mail
20. ☒ Other items or information:

Form PCT/IB/306; a postcard and a check in the amount of \$896.

Express Mail No. EK839852743US

Date of Deposit: December 18, 2000

U.S. APPLICATION NO. (IF KNOWN, SEE 37 CFR

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21. The following fees are submitted:

BASIC NATIONAL FEE (37 CFR 1.492 (a) (1) - (5)) :

- ☐ Neither international preliminary examination fee (37 CFR 1.482) nor international search fee (37 CFR 1.445(a)(2)) paid to USPTO and International Search Report not prepared by the EPO or JPO \$1,000.00
- ☒ International preliminary examination fee (37 CFR 1.482) not paid to USPTO but International Search Report prepared by the EPO or JPO \$860.00
- ☐ International preliminary examination fee (37 CFR 1.482) not paid to USPTO but international search fee (37 CFR 1.445(a)(2)) paid to USPTO \$710.00
- ☐ International preliminary examination fee paid to USPTO (37 CFR 1.482) but all claims did not satisfy provisions of PCT Article 33(1)-(4) \$690.00
- ☐ International preliminary examination fee paid to USPTO (37 CFR 1.482) and all claims satisfied provisions of PCT Article 33(1)-(4) \$100.00

ENTER APPROPRIATE BASIC FEE AMOUNT =**CALCULATIONS PTO USE ONLY**

\$860.00

Surcharge of \$130.00 for furnishing the oath or declaration later than ☐ 20 ☐ 30 months from the earliest claimed priority date (37 CFR 1.492 (e)).

\$0.00

CLAIMS	NUMBER FILED	NUMBER EXTRA	RATE	
Total claims	22 - 20 =	2	x \$18.00	\$36.00
Independent claims	3 - 3 =	0	x \$80.00	\$0.00
Multiple Dependent Claims (check if applicable).				<input type="checkbox"/> \$0.00

TOTAL OF ABOVE CALCULATIONS =

\$896.00

Reduction of 1/2 for filing by small entity, if applicable. Verified Small Entity Statement must also be filed (Note 37 CFR 1.9, 1.27, 1.28) (check if applicable).

☐

\$0.00

SUBTOTAL =

\$896.00

Processing fee of \$130.00 for furnishing the English translation later than ☐ 20 ☐ 30 months from the earliest claimed priority date (37 CFR 1.492 (f)).

+

\$0.00

TOTAL NATIONAL FEE =

\$896.00

Fee for recording the enclosed assignment (37 CFR 1.21(h)). The assignment must be accompanied by an appropriate cover sheet (37 CFR 3.28, 3.31) (check if applicable).

☐

\$0.00

TOTAL FEES ENCLOSED =

\$896.00

Amount to be:

refunded

\$

charged

\$

☒ A check in the amount of **\$896.00** to cover the above fees is enclosed.

☐ Please charge my Deposit Account No. _____ in the amount of _____ to cover the above fees.
A duplicate copy of this sheet is enclosed.

☒ The Commissioner is hereby authorized to charge any fees which may be required, or credit any overpayment to Deposit Account No. **02-4377** A duplicate copy of this sheet is enclosed.

NOTE: Where an appropriate time limit under 37 CFR 1.494 or 1.495 has not been met, a petition to revive (37 CFR 1.137(a) or (b)) must be filed and granted to restore the application to pending status.

SEND ALL CORRESPONDENCE TO:

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SIGNATURE

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NAME

32,300

REGISTRATION NUMBER

18 December 2000

DATE

09/11/99

PTO/PCT Rec'd 18 DEC 2000
Reaction Monitoring Systems

5 This invention relates to a method and apparatus for monitoring reactions and relates particularly, but not exclusively, to reactions which take place in DNA sequence determination.

10 There is a growing need today to be able to sequence efficiently large numbers of relatively short strands of DNA. A particularly useful method for doing this is the sequencing-by-synthesis method disclosed in WO 98/13523. In this method a complementary DNA strand is constructed using the normal rules of base pairings

15 to allow the sequence of the fragment of interest to be determined. Successive deoxynucleotides are added cyclically, but only the deoxynucleotide which is complementary to the base in the target position is incorporated into the growing complementary strand.

20 When a deoxynucleotide is incorporated, inorganic pyrophosphate (PPi) is released. The released PPi is converted to adenosine-triphosphate (ATP) by ATP sulfurylase. Luciferase is used to convert the ATP to adenosine monophosphate (AMP), PPi and light. The

25 luciferase reaction emits light at an intensity proportional to the concentration of ATP which is in turn dependent upon the amount of PPi produced and thus ultimately on the amount of deoxynucleotide incorporated. The light output may therefore be

30 detected and correlated with the incorporation of the particular deoxynucleotide present at that time.

Where the target sequence contains repetitions of a particular base, increased amounts of the complementary deoxynucleotide will be incorporated, leading to a

35 correspondingly increased emission of PPi which leads ultimately to an increased light intensity.

The reaction mixture also contains a nucleotide

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- 2 -

triphosphate degrading enzyme, apyrase. This enzyme degrades the excess remaining of the added deoxynucleotide and thereby circumvents the need for a wash cycle, that otherwise would be required to remove non-reacted deoxynucleotide between additions of the different deoxynucleotides. Apyrase also degrades the generated ATP and hence "turns off" the light from the reaction. Light emission reaches its maximum a few seconds after the addition of the deoxynucleotide, providing that it is complementary to the base in the next position of the template, and the enzymatic regeneration of the reaction is completed in approximately 60 seconds. Significant light is produced for approximately the first 30 seconds of the cycle and it is therefore desirable to follow the reaction for at least that period of time.

DNA sequencing performed according to the method described above is capable of generating high quality data in a simple fashion but the productivity of the method is not high if carried out as single reactions (typically 1 base read per 100 seconds).

From a first aspect the present invention provides an apparatus for simultaneously monitoring an array of reaction sites for light indicating that a reaction is taking place at a particular site, comprising an optically sensitive device arranged so that in use the light from a particular reaction site will impinge upon a particular predetermined region of said optically sensitive device, means for determining the light level impinging upon each of said predetermined regions and means to record the variation of said light level with time for each of said reaction sites.

Thus it will be seen that in accordance with the invention many potential reaction sites may be monitored at once with each site corresponding to a portion of the detection surface of the optically sensitive device. The optically sensitive device may then be scanned

- 3 -

periodically in a predetermined sequence to give an electrical signal corresponding to the light level emitted at each of the sites. In general, the predetermined regions corresponding to respective reaction sites will be distinct, although this is not necessarily true in all cases. This allows many reactions to be run in parallel thereby improving the productivity of preferred methods such as the one described above. Moreover, it is possible to monitor the automatic repetition of reactions, e.g. with successive deoxynucleotides in a target base identification process in which apyrase is used to break down unreacted deoxynucleotides between reactions. This follows because it is not necessary to carry out a separate result collection step after each reaction.

Such an apparatus has clear advantages for use in identifying a target base in a DNA sequence. This may for example be in order to determine the unknown sequence of a DNA strand or to screen for single nucleotide polymorphisms. In both cases, a target base may be identified in many samples at once, thereby drastically reducing the time taken to carry out the process for a given number of samples.

When viewed from a second aspect therefore, the invention provides an apparatus for identifying a target base in a DNA sequence comprising a plate having a plurality of reaction sites, an optically sensitive device arranged so that in use light from respective reaction sites signifying the incorporation of a nucleotide will impinge upon separate detection portions of said optically sensitive device, means for determining the level of light impinging upon said separate detection portions, thereby indicating the level of light emitted from each reaction site, and means for recording the variation of light output from each of said reaction sites with time.

It will also be appreciated that the invention

- 4 -

extends to a method of identifying a target base in a DNA sequence, comprising detecting the light level emitted from a plurality of reaction sites on respective portions of an optically sensitive device, converting the light impinging upon each of said portions of said optically sensitive device into an electrical signal which is distinguishable from the signals from all of said other regions, determining a light intensity for each of said discrete regions from the corresponding electrical signal, and recording the variations of said electrical signals with time.

Thus in accordance with the invention the progress of a plurality of light-emitting reactions may be monitored and recorded in real time. This enables a target base to be identified and thus is of particular benefit when used in the method disclosed in WO 98/13523, where deoxynucleotides may be added sequentially to a large number of reaction sites containing the target DNA and each can be monitored for the emission of light by the luciferase reaction while reagents are added to the remainder. This can significantly increase the efficiency of such a method.

It will be appreciated by those skilled in the art that the present invention is applicable both to the identification of a single target base in a DNA sequence e.g. when testing for a single base polymorphism and to the multiple repetition of such a method in order to sequence the target DNA.

The optically sensitive device may comprise an array of optical transducers - e.g. with each transducer corresponding to a subset of the reaction sites or even with an optical transducer corresponding to each reaction site. Preferably however the optically sensitive device comprises a single optical transducer. This is particularly advantageous in minimising the complexity of the optically sensitive device, and enabling a more compact design.

- 5 -

The reaction sites may be monitored from above, but preferably the reaction sites are monitored from underneath, with the parts of e.g. a plate beneath the reaction sites being at least partially transparent.

5 The reaction sites may simply be 'spots' of reagents on a flat plate which rely on surface tension. Preferably however the reaction sites are provided by wells in a reaction plate - e.g. a micro titre plate (MTP). In a particularly preferred embodiment many
10 reactions are run in parallel in an MTP. After having added a small amount of the first deoxynucleotide to the sample in the first well of the MTP, the time required to complete the cycle to the next addition for this well (reading the signal and degrading the excess of
15 deoxynucleotide) may be used to successively make addition of deoxynucleotides to the other samples of the MTP. Such an arrangement improves productivity, for example by two orders of magnitude (ie. one base read per second rather than one per 100 seconds), but it also
20 calls for a detection system capable of continuously reading the light intensity from a plurality of reactions.

25 The plate may simply be suspended or supported on a surface, which is transparent or semi-transparent where the reactions are monitored from below. Preferably however the plate is in contact with heat regulating means in order to maintain the plate at a substantially constant and uniform temperature.

30 In particularly convenient arrangements masking means are provided between the reaction sites to help to avoid cross-contamination of light between the reaction sites which can occur, particularly when the reaction sites are provided by wells.

35 This is novel and inventive in its own right and thus from a yet further aspect the present invention provides a reaction medium comprising a plurality of reaction sites which are partially transparent at a

- 6 -

lower part thereof, and opaque masking means between the reaction sites, said masking means being arranged so as to reduce the transmission of light between neighbouring reaction sites.

5 The masking means may comprise an opaque coating or the like applied selectively to the outer surfaces of said reaction sites so as to leave the lower parts thereof transparent or indeed the reaction sites may be made from two different materials, one of which is
10 opaque. Preferably however the masking means are provided by channels in a block - for example a temperature regulating block. The channels can advantageously serve to receive reaction sites in the form of wells. Channels in a block may also be useful
15 as masking means where the reaction sites are on a substantially flat plate rather than being an array of wells.

 Most preferably the channels flare outwardly towards the lower part thereof in order to maximise the
20 angles through which light may be emitted from the reaction sites or wells. It is also preferred that the masking means are at least partially reflective. Thus light which is initially emitted from reactions in a direction away from the optical path to the optically
25 sensitive device, can be redirected towards the optically sensitive device.

 In some embodiments of the invention light emitted from the reaction sites may impinge directly upon the optically sensitive device. In presently preferred
30 embodiments however, optical means are provided between the reaction sites and the optically sensitive device to direct light from respective reaction sites onto respective detection portions of the optically sensitive device. Advantageously the optical means allows the
35 optically sensitive device to be disposed remotely from the reaction sites. Said optical means may for example comprise a plurality of optical fibres - e.g. one per

- 7 -

reaction site to direct light onto the appropriate portion of the optically sensitive device. Such an arrangement has the advantage in that it allows a great flexibility in the placement of the optically sensitive device since a line of sight is not required.

In preferred embodiments the optical means comprises an array of lenses. Most preferably there is a lens for each reaction site to be monitored and the array has a layout substantially similar to the layout of the reaction sites being monitored. An array of lenses is a relatively inexpensive way to enhance the intensity of light impinging upon the optically sensitive device. Such an array can also minimise cross-contamination of light from adjacent reaction sites and thus improve the resolution of the system. The array of lenses may be arranged in exact correspondence with the array of reaction sites, i.e. with each lens being spaced from its neighbours by the same amount as the corresponding reaction site. More preferably however the centre-to-centre spacing of the lenses of such an array is smaller than the corresponding centre-to-centre spacing of the reaction sites. This is beneficial in affording a greater efficiency in the collection of light from the reaction sites at the periphery of the array since light from these sights must be slightly angled in order to focus the image of the lens array onto a light-sensitive device which is smaller than the lens array itself.

Any optically sensitive device capable of resolving the part of its sensitive surface upon which light impinges may be used, although preferably the optically sensitive device comprises a charge-coupled device (CCD). A CCD has a matrix of electrical potential wells, each of which represents a pixel. Light impinging upon these pixels is converted into an electric charge. An optical or mechanical shutter may be used to enable the charge at each pixel to be read

- 8 -

for each frame. However these add complexity to the apparatus and in the case of a mechanical shutter frequent repetitions for prolonged periods will mean a relatively short lifetime or expensive manufacture.

5 Preferably therefore a frame transfer CCD is used in which the charge at each pixel is stored in the respective electrical potential wells until a clocking signal moves the charge into corresponding non-light-sensitive storage areas for subsequent sequential
10 reading. A CCD is particularly preferred since it allows a relatively high light sensitivity together with a relatively high resolution so as to enable a large number of reaction sites to be monitored at relatively low cost.

15 The rate at which the optically sensitive device is read - ie. the sampling rate - is preferably such that the time between consecutive reads is less than or equal to the time between the addition of reagents to consecutive reaction sites, where applicable. This
20 ensures the correct monitoring of a plurality of reactions which are "triggered" at different times - e.g. by the addition of deoxynucleotides. Most preferably the sampling rate is sufficiently high to enable an evaluation of the kinetics of the reaction
25 being monitored - e.g. the rate of increase or decrease in light output, the total light energy given out (i.e. the area under the graph of light intensity against time) and the like. This is beneficial since in certain reactions such information is useful because it acts as
30 an indicator of the quality of the reaction. In certain convenient arrangements, where the invention is used in DNA sequencing, it is preferred that a measure of the total light energy output by a given reaction is determined in addition to or instead of the maximum
35 level of said light. This has been found to give a better indication of the number of bases incorporated than the maximum level or maximum level alone.

- 9 -

Preferably the electrical signals are converted into a digital signal prior to calculating the corresponding light intensity. Digital conversion offers the advantages of easy manipulation e.g. by a personal computer (PC) or dedicated hardware such as a digital signal processor (DSP).

The charge transferred from each pixel may be individually converted into a digital value by a suitable A/D converter. Preferably however the charges from a block of neighbouring pixels e.g. 5 by 5 pixels are added together to produce an aggregate signal for that block, the aggregate signal being fed to an A/D converter. This method increases the signal-to-noise ratio of the converted digital signal as compared to that for the conversion and subsequent addition of individual pixels.

Each predetermined region or detection portion of the optically sensitive device may correspond to a single pixel. Preferably however each corresponds to a plurality of pixels, most preferably a large number e.g. several hundred pixels. All of the blocks of pixels corresponding to a particular reaction site may then be added together to give a light intensity for that site. This technique can be used with the present invention since only a relatively few areas of light need to be detected - e.g. 96 if a 96 well MTP is used as in the most preferred embodiment.

A preferred embodiment of the present invention will now be described, by way of example only, and with reference to the accompanying drawings in which:

Fig. 1 is a graph of light intensity against time for a DNA sequence determination process which may be monitored in accordance with the present invention;

Fig. 2 is a schematic diagram of an embodiment of the present invention; and

Fig. 3 is a more detailed view of the lens array used in the embodiment of Figure 2.

- 10 -

Referring firstly to Fig. 1, a method of determining a DNA sequence 2 using the principle of sequencing-by-synthesis, will be briefly explained. A fuller explanation is given in WO 98/13523, although it is not essential for an understanding of the present invention.

A repeating series of adenine (A), guanine (G), thymine (T) and cytosine (C) deoxynucleotides are added at intervals of approximately one minute to the DNA fragment of interest which is a sequencing primer hybridized to a single stranded DNA fragment 6. A complementary strand 8 is successively built up in order to determine the sequence of the target 6. In the illustrated case the last base 8n of the complementary strand is a G. When A, G and T deoxynucleotides are successively added there is no significant reaction and therefore no significant light output. However when dCTP is added, the C nucleotide is incorporated since it complements the G base, 6n+1, which is the next in the target sequence. This incorporation is accompanied by a corresponding production of inorganic pyrophosphate which is converted into ATP by ATP sulfurylase which is already in the reaction mixture.

The ATP produced causes luciferase, also present, to emit light. This is shown on the graph by the left-most peak 10. This gives the first letter C in the determined sequence 2. The reaction mixture also contains a nucleotide triphosphate degrading enzyme, apyrase, that degrades the excess remaining of the added deoxynucleotide and thereby prepares the reaction mixture for the next cycle. Apyrase also degrades the generated ATP and hence "turns off" the light from the reaction. As may be seen, the cycle is repeated with the next nucleotide to be incorporated 4b being a T (to complement the A at 6n+2 in the target sequence).

It will be seen that when dATP is added at 4c, approximately twice as much light 12 is given off as

- 11 -

compared to the previous nucleotide incorporations.
This is explained by the fact that the target sequence
contains a repetition of the T base at 14. To
complement these, twice as much dATP is incorporated and
5 thus the DNA polymerase reaction gives twice as much
PPi.

It will be seen from the above that by constructing
the complementary strand 8, the sequence 2 is
determined, the complement of which gives the target
10 sequence 6.

Turning now to Figs. 2 and 3, an apparatus in
accordance with a preferred embodiment of the invention
is shown. The reactions of interest take place in the
wells of a 96 well MTP 14, which may be seen more
15 clearly in the enlarged fragment. The MTP 14 comprises
an array of wells 16 in an 8x12 configuration which is
moulded or vacuum formed from a suitable transparent
plastics material. For convenience the whole MTP 14 is
made from the same material although alternatively just
20 the base 18 may be transparent. In the embodiment
described, the thickness of the well walls 20 is
approximately 0.3 mm.

The wells 16 are received in channels 22 in a
heating block 24 which is made of aluminium so as to
25 have a high reflectance for visible light. The walls of
the channels 22 taper downwardly from the top although
flare out at the bottom end 20 in order to avoid
obscuring light emitted through the well.

The DNA samples to be analysed are placed in the
30 respective wells 16 and the MTP is then located in the
apparatus, where the reagents 48 are added by a
dispenser 50 which is computer-controlled to deliver a
precise volume of the required reagent from a reagent
cassette (not shown). The dispenser 50 is moved across
35 the MTP 14 by means of an x-y table 52. Alternatively
the reagents may be pre-dispensed, e.g. manually, into
the wells, before the MTP is placed in the apparatus.

- 12 -

Below the MTP 14 by a distance of 9 mm is a lens array 26. As may be seen from the detail view, the lens array 26 is arranged so that there is a separate lens 28 below each well 16 in the MTP. However the centre-to-centre spacings of the lenses 28 are all 8.75 mm, whereas the centre-to-centre spacings of the wells 16 are all 9.0 mm. This difference in the respective spacings of the wells 16 and lenses 28 emulates the effect of a field lens to reduce the difference in efficiency of light collection between the wells in the centre of the MTP and those at the periphery. The areas 30 between the lenses 28 are opaque and so will be detected as dark areas by the camera. The lens array is such that light coming down at any angle from reactions in the wells 16 will pass through the lens 28 or will be absorbed by the opaque area 30 rather than entering an adjacent lens. The possibility of cross-contamination of light between the wells 16 is thereby avoided.

Vertically below the lens array 26 is a mirror 32 inclined at approximately 45° to deflect light horizontally. Further along the optical path is a CCD camera 34. The camera has a lens 36 which focuses incoming light onto the CCD chip 38 inside the camera. The CCD chip 38 is a frame-transfer CCD chip and has 500x290 charge elements. Each of the charge elements of the CCD chip corresponds to a pixel and develops a charge when illuminated proportional to the intensity of the incident light. A clock signal of approximately 1 Hz is generated by a suitable oscillator in order to shift charges from the light sensitive elements to positions within the chip which are screened from light. During the interval between the main clock pulses, the charges of blocks of 5x5 pixels are added together in a process called binning which is carried out by 'binning' circuit 40. The aggregate values are then converted to a digital format by an analogue to digital convertor 42. A further analysis stage 44 correlates the digital

- 13 -

signals for the blocks with corresponding wells 14 on the MTP and adds the values of all the blocks for a given well together. In the desired example in which each block is made up of 5x5 pixels there will be a potential total of 5800 blocks. As the MTP has 96 wells there is a potential maximum of 60 blocks per well. In practice some blocks will correspond to the gaps between the wells and each well will be associated with fewer blocks. A serial connection carries the data to a PC for recording and displaying the light intensity for each well. The results may be displayed in any convenient format. For example a graph such as the one shown in Fig. 1 may be displayed or be available for display for each well 16.

Although the data connection 46 to a PC is shown after the binning 40, A/D conversion 42 and addition 44 stages, alternative arrangements are possible. For example some or all of these stages may be performed within the PC. Further processing may also be performed in the PC e.g. a pre-screening designed only to display the light outputs corresponding nucleotide incorporations - i.e. to apply a threshold light level. Indeed this may be implemented at an earlier stage in the system such as the CCD or associated circuitry to record the light output only during an incorporation event when the level is above a predefined threshold.

It will be appreciated by those skilled in the art that whilst a process of determining an unknown DNA sequence has been described, the invention may be used equally for identifying single nucleotide polymorphisms for example.

25-08-2000

- 14 -

Claims

1. An apparatus for simultaneously monitoring an array of reaction sites for light indicating that a reaction is taking place at a particular site, comprising:
- 5 means for receiving a plurality of liquid samples at respective reaction sites;
- means for dispensing at least one reagent into said samples;
- 10 an optically sensitive device arranged so that in use the light generated by the reaction of a particular liquid sample will impinge upon a particular predetermined region of said optically sensitive device;
- means for determining the level of light impinging
- 15 upon each of said predetermined regions; and
- means to record the variation of said light level with time for each of said liquid samples.
2. An apparatus as claimed in claim 1, wherein said
- 20 means for receiving a plurality of liquid samples comprises a plate.
3. An apparatus for identifying target bases in DNA sequences comprising:
- 25 a plate for receiving a plurality of liquid samples at respective reaction sites;
- means for dispensing at least one reagent into said samples;
- an optically sensitive device arranged so that in
- 30 use light generated by the reaction of a particular liquid sample signifying the incorporation of a nucleotide will impinge upon a particular region of said optically sensitive device;
- means for determining the level of light impinging
- 35 upon each of said said predetermined regions; and
- means for recording the variation of said light level with time.

AMENDED SHEET

- 15 -

4. An apparatus as claimed in claim 1, 2 or 3, wherein the optically sensitive device comprises a single optical transducer.
5. An apparatus as claimed in claim 1, 2, 3 or 4, arranged to monitor the reaction sites from underneath.
6. An apparatus as claimed in any of claims 1 to 5, comprising an array of lenses between, or arranged in use between, said reaction sites and the optically sensitive device.
7. An apparatus as claimed in claim 6, wherein the lenses of said array are spaced by a smaller amount than the spacing of the corresponding reaction sites.
8. An apparatus as claimed in any preceding claim, wherein the optically sensitive device comprises a charge-coupled device.
9. An apparatus as claimed in claim 8, wherein the optically sensitive device comprises a frame transfer charge-coupled device.
10. An apparatus as claimed in any preceding claim, comprising means to record a measure of the total light output from a given reaction site.
11. An apparatus as claimed in any preceding claim, comprising means to convert the electrical output from said optically sensitive device into a digital signal.
12. An apparatus as claimed in claim 11, wherein said conversion means converts the signals from a plurality of neighbouring pixels in a single block.
13. An apparatus as claimed in any of claims 2 to 12,

AMENDED SHEET

25-08-2000

- 16 -

wherein said plate is in contact with heat regulating means.

14. An apparatus as claimed in any of claims 2 to 13,
5 wherein masking means are provided between reaction sites on the plate.

15. An apparatus as claimed in claim 14, wherein said masking means are provided by channels in a block.

10 16. An apparatus as claimed in claim 15, wherein said block comprises temperature regulating means.

15 17. An apparatus as claimed in claim 15 or 16, wherein said channels flare outwardly towards the lower part thereof.

20 18. A method of identifying a target base in a DNA sequence, comprising detecting the light level emitted from a plurality of reaction sites on respective portions of an optically sensitive device, converting the light impinging upon each of said portions of said optically sensitive device into an electrical signal which is distinguishable from the signals from all of
25 said other regions, determining a light intensity for each of said discrete regions from the corresponding electrical signal, and recording the variations of said electrical signals with time.

30 19. A method as claimed in claim 18, comprising monitoring a plurality of reaction sites simultaneously.

20. A method as claimed in claim 18 or 19, wherein the
35 interval between successive readings of the state of the optically sensitive device is less than or equal to the time between the addition of reagents to consecutive reaction sites.

AMENDED SHEET

25-08-2000

- 17 -

which is distinguishable from the signals from all of said other regions, determining a light intensity for each of said discrete regions from the corresponding electrical signal, and recording the variations of said electrical signals with time.

20. A method as claimed in claim 19, comprising monitoring a plurality of reaction sites simultaneously.

21. A method as claimed in claim 19 or 20, wherein the interval between successive readings of the state of the optically sensitive device is less than or equal to the time between the addition of reagents to consecutive reaction sites.

22. A method as claimed in any of claims 18 to 21 comprising recording the times at which a series of peaks in light output occur for each sample and, thereby enabling each peak to be associated with the addition of a particular reagent to the corresponding sample.

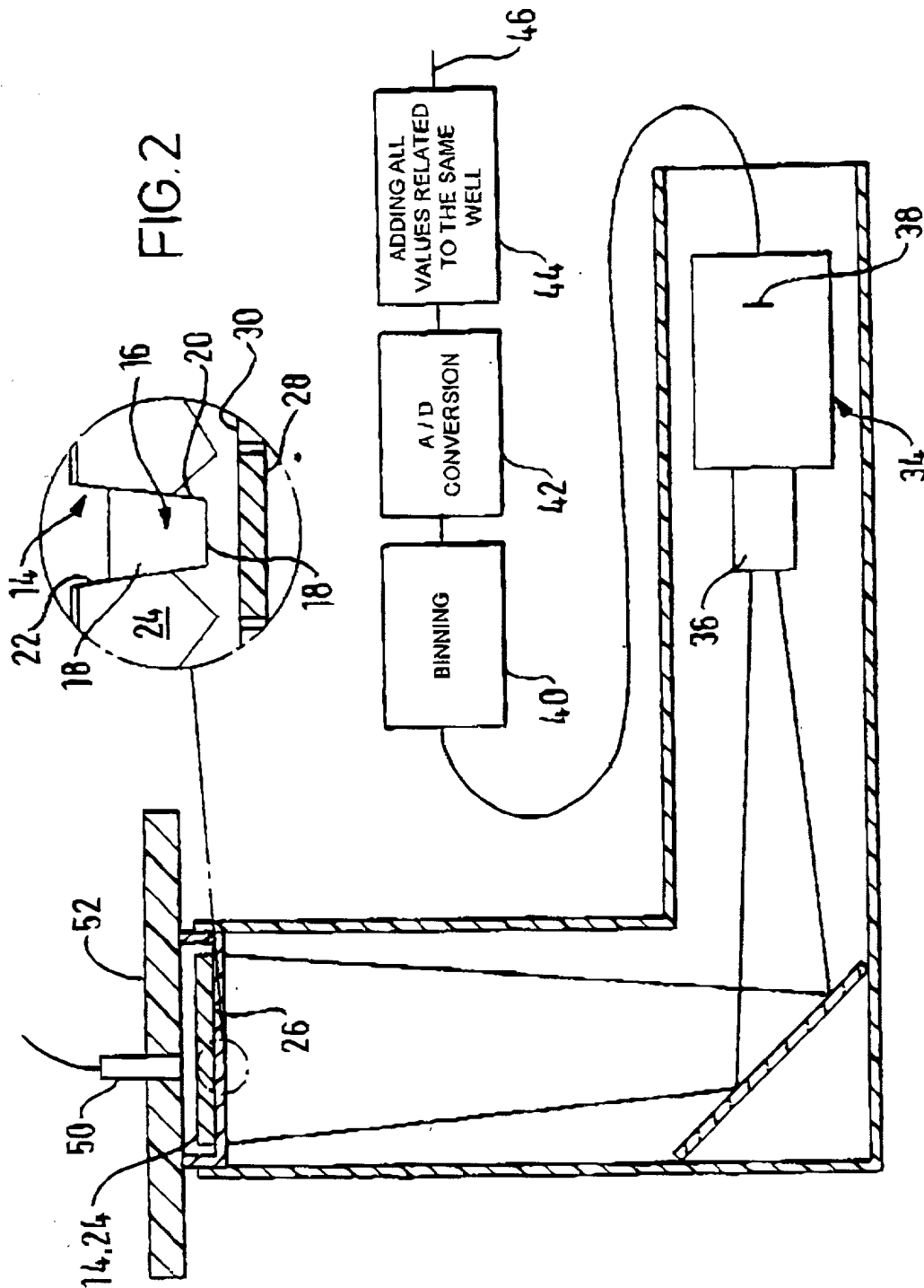
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SUBSTITUTE SHEET (RULE 26)

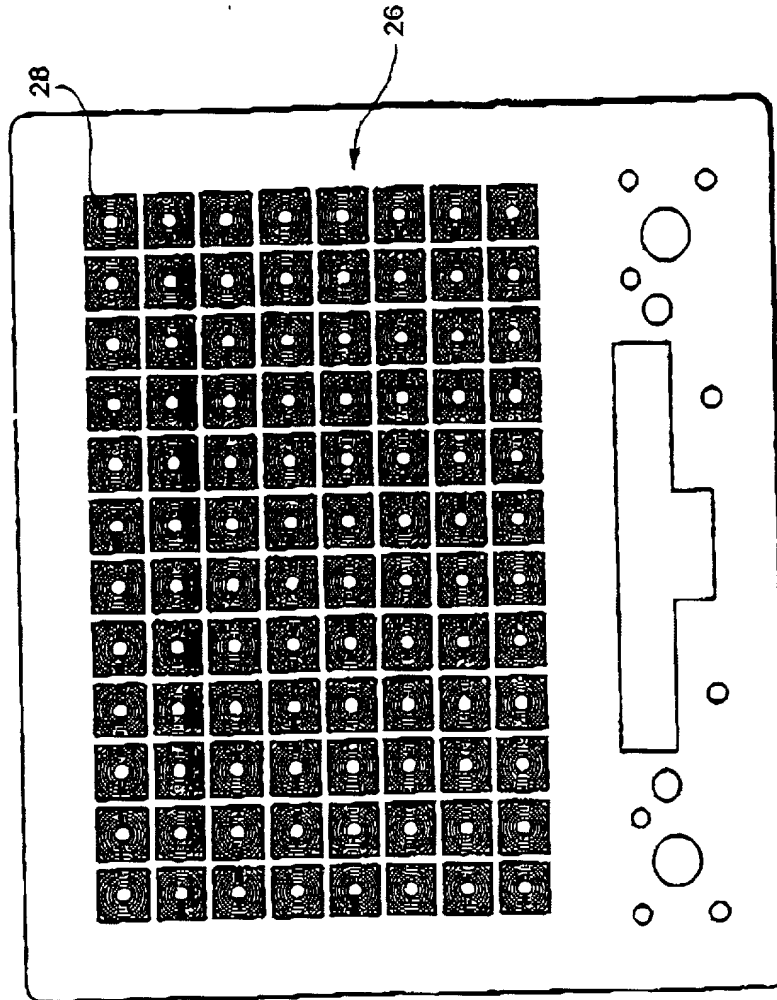
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FIG. 3



SUBSTITUTE SHEET (RULE 26)



FILE NO.A33846-PCT-USA-072745.0116

PATENT

PTO PCT Rec'd 14 JUN 2001

IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

Applicant : Hagerlid et al.
Serial No. : 09/719,960 Examiner : Not Yet Assigned
Filed : December 18, 2000 Group Art Unit: Not Yet Assigned
For : REACTION MONITORING SYSTEM

PRELIMINARY AMENDMENT

I hereby certify that this paper is being deposited
with the United States Postal Service as first class mail in
an envelope addressed to: Assistant Commissioner for
Patents, Washington, D.C. 20231

June 11, 2001
Date of Deposit

Janet M. MacLeod
Attorney Name

35,263
PTO Registration No

Janet M MacLeod
Signature

June 11, 2001
Date of Signature

Assistant Commissioner for Patents

Washington, D.C. 20231

Sir:

Prior to examination of the above-identified application, please enter the following amendment and consider the following remarks.

IN THE CLAIMS:

Please cancel Claims 1-22 without prejudice.

Please add the following claims:

(New) 23. An apparatus for simultaneously monitoring an array of reaction sites for light indicating that a reaction is taking place at a particular site, comprising:

means for receiving a plurality of liquid samples at respective reaction sites;

means for dispensing at least one reagent into said samples;

an optically sensitive device arranged so that in use the light sample will impinge upon a particular predetermined region of said optically sensitive device;

means for determining the level of light impinging upon each of said predetermined regions; and

means to record the variation of said light level with time for each of said liquid samples.

(New) 24. An apparatus as claimed in Claim 23, wherein said means for receiving a plurality of liquid samples comprises a plate.

(New) 25. An apparatus for identifying target bases in DNA sequences comprising:

a plate for receiving a plurality of liquid samples at respective reaction sites;

means for dispensing at least one reagent into said samples;

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an optically sensitive device arranged so that in use light generated by the reaction of a particular liquid sample signifying the incorporation of a nucleotide will impinge upon a particular region of said optically sensitive device;

means for determining the level of light impinging upon each of said predetermined regions; and

means for recording the variation of said light level with time.

(New) 26. An apparatus as claimed in Claim 23 wherein the optically sensitive device comprises a single optical transducer.

(New) 27. An apparatus as claimed in Claim 23 arranged to monitor the reaction sites from underneath.

(New) 28. An apparatus as claimed in Claim 23, comprising an array of lenses between, or arranged in use between, said reaction sites and the optically sensitive device.

(New) 29. An apparatus as claimed in Claim 28, wherein the lenses of said array are spaced by a smaller amount than the spacing of the corresponding reaction sites.

(New) 30. An apparatus as claimed in Claim 23, wherein the optically sensitive device comprises a charge-coupled device.

(New) 31. An apparatus as claimed in Claim 30, wherein the optically sensitive device comprises a frame transfer charge-coupled device.

(New) 32. An apparatus as claimed in Claim 23, comprising means to record a measure of the total light output from a given reaction site.

(New) 33. An apparatus as claimed in Claim 23, comprising means to convert the electrical output from said optically sensitive device into a digital signal.

(New) 34. An apparatus as claimed in Claim 33, wherein said conversion means converts the signals from a plurality of neighbouring pixels in a single block.

(New) 35. An apparatus as claimed in Claim 24, wherein said plate is in contact with heat regulating means.

(New) 36. An apparatus as claimed in Claim 24, wherein masking means are provided between reaction sites on the plate.

(New) 37. An apparatus as claimed in Claim 36, wherein said masking means are provided by channels in a block.

(New) 38. An apparatus as claimed in Claim 37, wherein said block comprises temperature regulating means.

(New) 39. An apparatus as claimed in Claim 37, wherein said channels flare outwardly towards the lower part thereof.

(New) 40. A method of identifying a target base in a DNA sequence, comprising detecting the light level emitted from a plurality of reaction sites on respective portions of an optically sensitive device, converting the light impinging upon each of said portions of said optically sensitive device into an electrical signal which is distinguishable from the signals from all of said other regions, determining a light intensity for each of said discrete regions from the corresponding electrical signal, and recording the variations of said electrical signals with time.

(New) 41. A method as claimed in Claim 40, comprising monitoring a plurality of reaction sites simultaneously.

(New) 42. A method as claimed in Claim 40, wherein the interval between successive readings of the state of the optically sensitive device is less than or equal to the time between the addition of reagents to consecutive reaction sites.

(New) 43. A method as claimed in Claim 41, comprising monitoring a plurality of reaction sites simultaneously.

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(New) 44. A method as claimed in Claim 41, wherein the interval between successive readings of the state of the optically sensitive device is less than or equal to the time between the addition of reagents to consecutive reaction sites.

(New) 45. A method as claimed in Claim 40, comprising recording the times at which a series of peaks in light output occur for each sample and, thereby enabling each peak to be associated with the addition of a particular reagent to the corresponding sample.

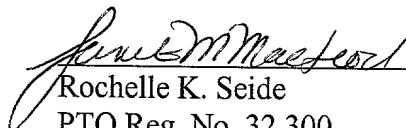
REMARKS

The Notification of Missing Requirements mailed February 9, 2001 for the above-identified application indicates that Preliminary Amendment filed December 18, 2000 "doesn't match claims."

The Preliminary Amendment filed December 18, 2000 amends the claims in this national stage application which were previously amended under Article 34 in the international stage on August 25, 2000. Applicants believe that the Preliminary Amendment of December 18, 2000 is appropriately directed to the claims pending on that date. However, in the interest of avoiding confusion, all pending claims have been canceled without prejudice. New Claims 23-45 have been added, and represent the claims of the international application amended to remove multiple dependencies. Accordingly, the present amendment does not change the scope of the claims, but merely renumbers the claims.

Favorable reconsideration and allowance of all pending claims is earnestly solicited.

Respectfully submitted,


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Janet M. MacLeod
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IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

Applicants : HAGERLID, Peter et al.
Serial No. : To be assigned
Filed : 18 December 1999
For : REACTION MONITORING SYSTEMS

Express Mail Mailing No. EK839852743US

PRELIMINARY AMENDMENT

Assistant Commissioner of Patent
Box PCT
Washington, D.C., 20231

Sir or Madam:

Prior to examination of the above-identified application, please make the following amendments:

IN THE CLAIMS:

Please cancel Claims 28 to 31 without prejudice.

Claim 4, Line 1: please delete "2 or 3,".

Claim 5, Line 5: please delete "2, 3 or 4".

Claim 6, Line 8: please delete "any of claims 1 to 5" and substitute therefor --claim 5--.

Claim 8, Line 17: please delete "any preceding claim" and substitute therefor --claim 7--.

Claim 10, Line 25: please delete "any preceding claim" and substitute therefor --claim 9--.

- Claim 11, Line 29: please delete "any preceding claim" and substitute therefor --claim 10--.
- Claim 13, Line 36: please delete "any of claims 2 to 12" and substitute therefor --claim 12--.
- Claim 14, Line 4: please delete "any of claims 2 to 13" and substitute therefor --claim 13--.
- Claim 17, Line 14: please delete "15 or".
- Claim 20, Line 33: please delete "18 or".
- Claim 21, Line 10: please delete "19 or".
- Claim 22, Line 16: please delete "any of claims 18 to 21" and substitute therefor --claim 21--.

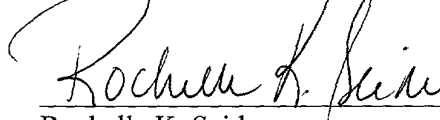
REMARKS

The claims have been amended to remove multiple dependencies. No new matter has been introduced by this amendment.

Favorable consideration and allowance of all pending claims is earnestly solicited.

Respectfully submitted,

BAKER BOTTS LLP



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Dated: December 18, 2000

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BAKER BOTTS LLP.
FILE NO. A33846-PCT-USA-072745.0116

COMBINED DECLARATION
AND POWER OF ATTORNEY

(Original, Design, National Stage of PCT, Divisional, Continuation or C-I-P Application)

As a below named inventor, I hereby declare that:
My residence, post office address and citizenship are as stated below next to my name; I believe I am the original,
first and sole inventor (if only one name is listed below) or an original, first and joint inventor (if plural names are
listed below) of the subject matter which is claimed and for which a patent is sought on the invention entitled:

REACTION MONITORING SYSTEM

This declaration is of the following type:

- ☐ original
- ☐ design
- ☒ national stage of PCT.
- ☐ divisional
- ☐ continuation
- ☐ continuation-in-part (C-I-P)

the specification of which: *(complete (a), (b), or (c))*

- (a) ☐ is attached hereto.
- (b) ☒ was filed on December 18, 2000, as Application Serial No. 09/719,960 and was amended on *(if applicable)*.
- (c) ☒ was described and claimed in PCT International Application No. PCT/GB99/01834 filed on June 18, 1999 and was amended on *(if applicable)*.

Acknowledgement of Review of Papers and Duty of Candor

I hereby state that I have reviewed and understand the contents of the above identified specification, including the claims, as amended by any amendment referred to above.

I acknowledge the duty to disclose information which is material to the patentability of the subject matter claimed in this application in accordance with Title 37, Code of Federal Regulations § 1.56.

☐ In compliance with this duty there is attached an information disclosure statement 37 CFR 1.98.

Priority Claim

I hereby claim foreign priority benefits under Title 35, United States Code, § 119(a)-(d) of any foreign application(s) for patent or inventor's certificate or of any PCT International Application(s) designating at least one country other than the United States of America listed below and have also identified below any foreign application(s) for patent or inventor's certificate or any PCT International Application(s) designating at least one country other than the United States of America filed by me on the same subject matter having a filing date before that of the application on which priority is claimed

(complete (d) or (e))

- (d) ☐ no such applications have been filed.
- (e) ☒ such applications have been filed as follows:

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BAKER BOTTS L.L.P.

FILE NO. A33846-PCT-USA-072745.0116

PRIOR FOREIGN/PCT APPLICATION(S) FILED WITHIN 12 MONTHS (6 MONTHS FOR DESIGN) PRIOR TO SAID APPLICATION			
COUNTRY	APPLICATION NO.	DATE OF FILING (day, month, year)	DATE OF ISSUE (day, month, year)
Great Britain	981321610	June 18, 1998	
ALL FOREIGN APPLICATION(S), IF ANY, FILED MORE THAN 12 MONTHS (6 MONTHS FOR DESIGN) PRIOR TO SAID APPLICATION			

Claim for Benefit of Prior U.S. Provisional Application(s)

I hereby claim the benefit under Title 35, United States Code, § 119(e) of any United States provisional application(s) listed below:

Provisional Application Number	Filing Date

Claim for Benefit of Earlier U.S./PCT Application(s) under 35 U.S.C. 120

(complete this part only if this is a divisional, continuation or C-I-P application)

I hereby claim the benefit under Title 35, United States Code, § 120 of any United States application(s) or PCT international application(s) designating the United States of America that is/are listed below and, insofar as the subject matter of each of the claims of this application is not disclosed in the prior application(s) in the manner provided by the first paragraph of Title 35, United States Code § 112, I acknowledge the duty to disclose information as defined in Title 37, Code of Federal Regulations, § 1.56 which occurred between the filing date of the prior application(s) and the national or PCT international filing date of this application:

(Application Serial No.)	(Filing Date)	(Status) (patented, pending, abandoned)

Power of Attorney

As a named inventor, I hereby appoint Dana M. Raymond, Reg. No. 18,548; Frederick C. Carver, Reg. No. 17,021; Francis J. Hone, Reg. No. 18,662; Joseph D. Garon, Reg. No. 20,420; Arthur S. Tenser, Reg. No. 18,839; Ronald B. Hildreth, Reg. No. 19,498; Thomas R. Nesbitt, Jr., Reg. No. 22,075; Robert Nemer, Reg. No. 24,316; Richard G. Berkley, Reg. No. 25,465; Richard S. Clark, Reg. No. 26,154; Bradley B. Geist, Reg. No. 27,551; James J. Maune, Reg. No. 26,946; John D. Murman, Reg. No. 29,836; Henry Tang, Reg. No. 29,705; Robert C. Schneinfeld, Reg. No. 31,300; John A. Fogarty, Jr., Reg. No. 22,848; Louis S. Sorrell, Reg. No. 32,439; Rochelle K. Seide Reg. No. 32,300; Gary M. Butter, Reg. No. 33,841; Marta E. Delsignore, Reg. No. 32,689; and Lisa B. Kole, Reg. No. 35,225 of the firm of BAKER BOTTS L.L.P., with offices at 30 Rockefeller Plaza, New York, New York 10112, as attorneys to prosecute this application and to transact all business in the Patent and Trademark Office connected therewith.

SEND CORRESPONDENCE TO:
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(212) 705-5000

I hereby declare that all statements made herein of my own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under Section

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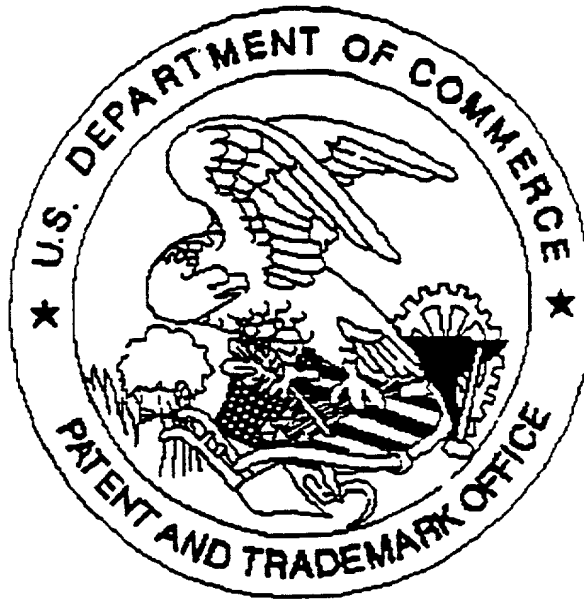
BAKER BOTTS LLP.

FILE NO.: A33846-PCT-USA-072745.0116.

1001 of Title 18 of the United States Code and that such willful false statements may jeopardize the validity of the application or any patent issued thereon.

FULL NAME OF SOLE OR FIRST INVENTOR	LAST NAME HAGERLID	FIRST NAME PETER	MIDDLE NAME
RESIDENCE & CITIZENSHIP	CITY UPPSALA	STATE or FOREIGN COUNTRY SWEDEN	COUNTRY OF CITIZENSHIP SWEDEN
POST OFFICE ADDRESS	POST OFFICE ADDRESS SKOLDUNGAGATAN 1	CITY UPPSALA	STATE or COUNTRY SWEDEN
DATE 3 June 2001	SIGNATURE OF INVENTOR <i>[Signature]</i>		
FULL NAME OF SECOND JOINT INVENTOR, IF ANY	LAST NAME EKSTROM	FIRST NAME Björn	MIDDLE NAME
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DATE 8 June 2001	SIGNATURE OF INVENTOR <i>[Signature]</i>		
FULL NAME OF THIRD JOINT INVENTOR, IF ANY	LAST NAME SIOBERG	FIRST NAME Jonas	MIDDLE NAME
RESIDENCE & CITIZENSHIP	CITY UMEÅ	STATE or FOREIGN COUNTRY SWEDEN	COUNTRY OF CITIZENSHIP SWEDEN
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DATE 8 June 2001	SIGNATURE OF INVENTOR <i>[Signature]</i>		
FULL NAME OF FOURTH JOINT INVENTOR, IF ANY	LAST NAME	FIRST NAME	MIDDLE NAME
RESIDENCE & CITIZENSHIP	CITY	STATE or FOREIGN COUNTRY	COUNTRY OF CITIZENSHIP
POST OFFICE ADDRESS	POST OFFICE ADDRESS	CITY	STATE or COUNTRY
DATE	SIGNATURE OF INVENTOR		
FULL NAME OF FIFTH JOINT INVENTOR, IF ANY	LAST NAME	FIRST NAME	MIDDLE NAME
RESIDENCE & CITIZENSHIP	CITY	STATE or FOREIGN COUNTRY	COUNTRY OF CITIZENSHIP
POST OFFICE ADDRESS	POST OFFICE ADDRESS	CITY	STATE or COUNTRY
DATE	SIGNATURE OF INVENTOR		
FULL NAME OF SIXTH JOINT INVENTOR, IF ANY	LAST NAME	FIRST NAME	MIDDLE NAME
RESIDENCE & CITIZENSHIP	CITY	STATE or FOREIGN COUNTRY	COUNTRY OF CITIZENSHIP
POST OFFICE ADDRESS	POST OFFICE ADDRESS	CITY	STATE or COUNTRY
DATE	SIGNATURE OF INVENTOR		

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